

# In vitro model of prepacked CO<sub>2</sub> absorber use: development and testing

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## Introduction

The canister life of prepacked CO<sub>2</sub> absorbents has been studied in vitro for various brands over a range of fresh gas flows (FGF) using a metric called ‘fractional canister usage’ or FCU<sup>[1]</sup>. FCU is the reciprocal of the time (in hours) for the inspiratory CO<sub>2</sub> fraction (F<sub>I</sub>CO<sub>2</sub>) to reach 0.5% (= the fraction of total canister life used per hour). The FGF - FCU relationship, previously found to be linear, has only been tested with a 160 mL/min CO<sub>2</sub> load (VCO<sub>2</sub>) and 5 L/min minute ventilation (MV). We now extend the model to include the effects of VCO<sub>2</sub>, target end-tidal CO<sub>2</sub> fraction (F<sub>ET</sub>CO<sub>2</sub>), MV, and dead-space ventilation (V<sub>D</sub>).

## Methods

We derived 4 models from first principles (see Figure 1) and tested them prospectively in vitro. In model A and B, MV was derived from spirometry, in model C and D from the alveolar air equation (Nunn):  $MV = (VCO_2/F_{ET}CO_2)/(1-fVD)$ , with fVD (dead space fraction) = 0.29, calculated with Bohr’s formula:  $fVD = (F_{ET}CO_2 - F_{ME}CO_2)/F_{ET}CO_2$ , with F<sub>ME</sub>CO<sub>2</sub> = mixed-expired FCO<sub>2</sub> determined using a mixing bottle. In models B and D, an additional parameter (machine factor), allowing the intercept with the FGF to differ from MV, was empirically determined using Excel’s solver function: minimization of squared differences between modeled and observed FCU.

Canisters (Medisorb, Molecular Products, UK, lot # LO1A-00903) were inserted into an Aisys machine (GE, Madison, WI) ventilating a 2 L bag with a known VCO<sub>2</sub> into its tip. To test whether the FCU intercept of the FGF - FCU curve varied proportionally with VCO<sub>2</sub>, FCU of 5 canisters was determined with either 80, 120, 160, 240 and 320 mL/min VCO<sub>2</sub> while adjusting MV to 4.2% F<sub>ET</sub>CO<sub>2</sub> with a 0.3 L/min FGF, and linear regression applied to the data. To test whether the FCU intercept was independent of MV, the measurements were repeated with a constant MV (5 L/min) and a paired t-test was performed to compare FCU values amongst this and the previous experiment (p < 0.05 denoting statistical significance). Secondly, we hypothesized that an increase in VCO<sub>2</sub> accompanied by a (proportional) increase in MV to keep F<sub>ET</sub>CO<sub>2</sub> constant would shift the straight line describing the FGF-FCU relationship in a parallel manner. To test this, FCU was determined for 19 canisters with different combinations of VCO<sub>2</sub> (80, 160, 240 and 320 mL/min) and FGF (range 0.3 - 5L/min); MV was adjusted to maintain F<sub>ET</sub>CO<sub>2</sub>. Model performance when compared to observed FCU was assessed using Varvel’s criteria<sup>[2]</sup>, median performance error (MDPE) and median absolute performance error (MDAPE).

## Results

FCU is proportional with VCO<sub>2</sub> and independent of ventilation (constant F<sub>A</sub>CO<sub>2</sub> group:  $FCU = VCO_2 * 0.046 - 0.87$ ; r<sup>2</sup> = 1.00 ; constant MV group:  $FCU = VCO_2 * 0.048 - 1.32$ ; r<sup>2</sup> = 1.00). VCO<sub>2</sub>-FCU pairs did not differ between the 2 groups (p = 0.96) indicating that FCU intercept is ventilation independent. Of the 4 models, model B and D performed best (see Figure 1) and confirmed the hypothesized parallel shift.

## Discussion

Over a 20-100% rebreathing range, the FCU-FGF models that allow the FGF intercept to deviate from MV by introducing the machine factor performed very well, with only small deviations from linearity during high FGF and VCO<sub>2</sub> extremes. Why the FGF intercept is lower than MV remains speculative but is possibly related to machine specific flow dynamics. These models will help us determine the economic and ecologic impact of anesthesia.

## References

- Hendrickx JF, De Ridder SP, Dehouwer A, Carette R, De Cooman S, De Wolf AM. In

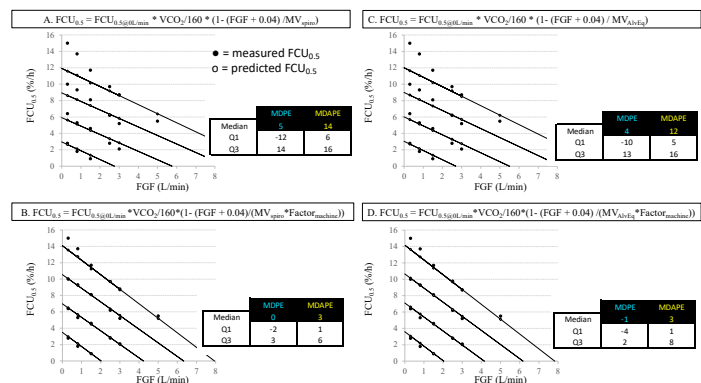


Figure 1 Four models derived from first principles and tested in vitro

vitro performance of prefilled CO<sub>2</sub> absorbers with the Aisys®. J Clin Monit Comput  
2016;30:193-202

2. Varvel JR, Donoho DL, Shafer SL. Measuring the predictive performance of computer-controlled infusion pumps. J Pharmacokinet Biopharm. 1992 Feb;20(1):63-94.